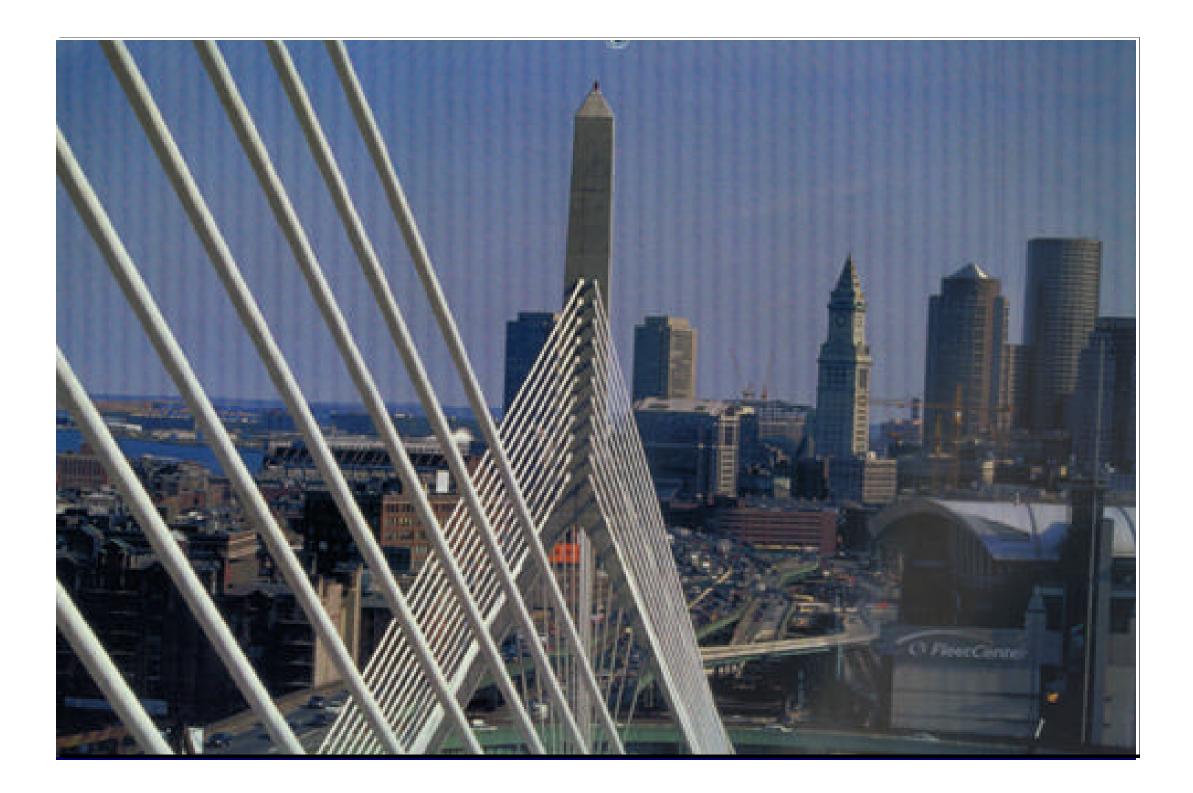
MANAGING PATIENT DOSE IN FLUOROSCOPIC PROCEDURES

Keith J. Strauss, MSc, FAAPM Director, Radiology Physics & Engineering Children's Hospital Harvard Medical School







DILEMAS

- **A. Fluoroscopically Guided Interventions**
 - 1. Minor
 - 2. Life Saving
- **B.** Deterministic Injuries
 - 1. None
 - 2. Severe
- C. Responsible Physician Must Choose to Continue or Stop Complex Interventions





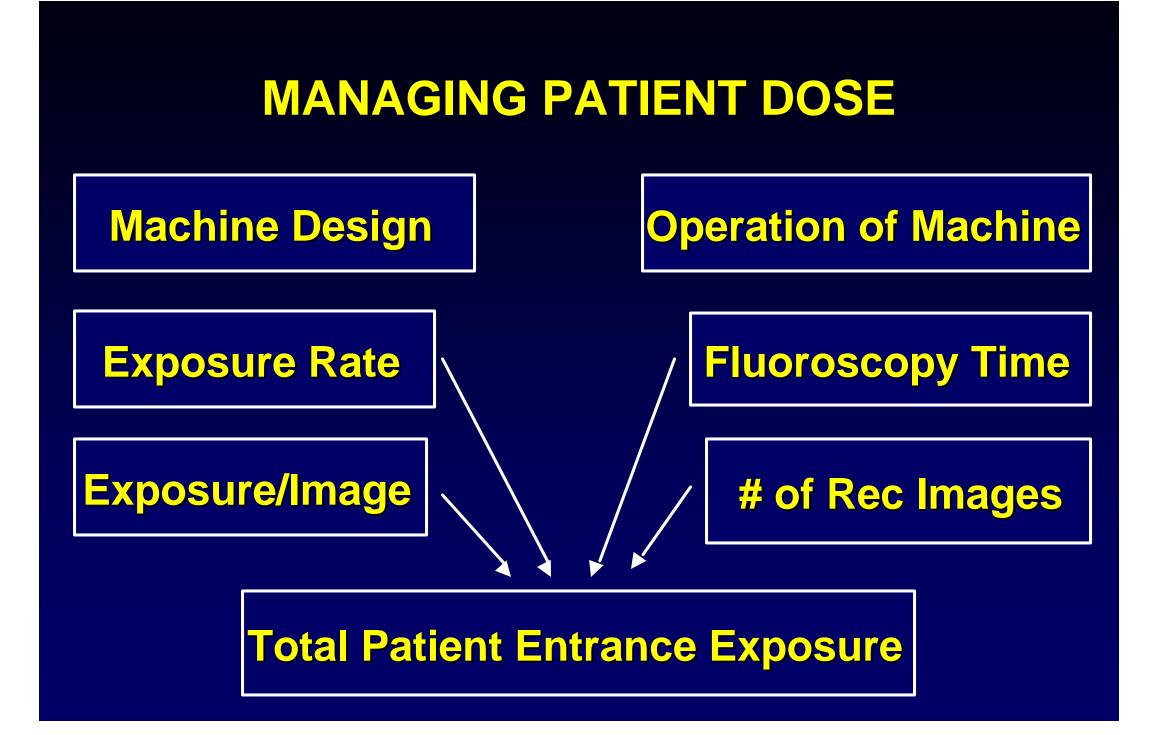
D. <u>Real-Time</u> Data Needed to Balance

- 1. Radiation Risk
- 2. Clinical Benefit

E. Physician Hand Cuffed by:

- **1. Regulatory Total Dose Limits**
- 2. Inappropriately Applied Reference Levels







F. Is <u>Real-Time</u> Data Over Kill?

- 1. Adults
 - a. Complex Interventions
 - **b.** Routine Interventions may not Require
- **2. All Pediatric Cases**
 - a. Elevated Radiosensitivity
 - **b.** Multiple Follow Up Procedures

INTRODUCTION

A. Requirements of Patient Exam **B.** Imaging Equipment Design Must be **Exploited** to Minimize Patient Dose **C. Acceptance Testing** D. Training of Staff E. Real-Time Dose Monitoring Techniques



A. Organ System(s) Studied

- 1. Vascular
 - a. Heart
 - **b.** Arterial
 - c. Venous
- 2. Nonvascular
 - A. Digestive Tract
 - **B.** Drainages/Punctures



B. Patient Size Affects:

- **1. Image Quality Requirements**
- 2. Patient Sensitivity to Radiation
- 3. Patient Dose
- 4. Required Ancillary Support
 - a. Equipment
 - **b.** Additional Staff



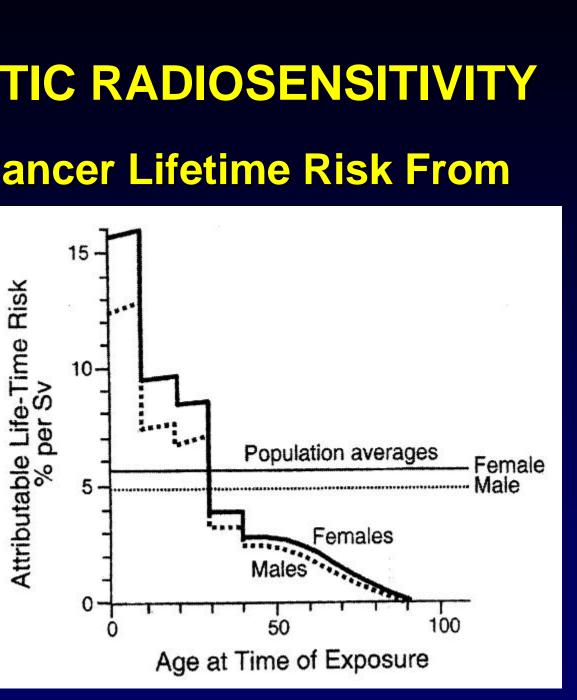
PATIENT STOCHASTIC RADIOSENSITIVITY

C. Radiation Induced Cancer Lifetime Risk From

1 Sv Whole Body

Dose

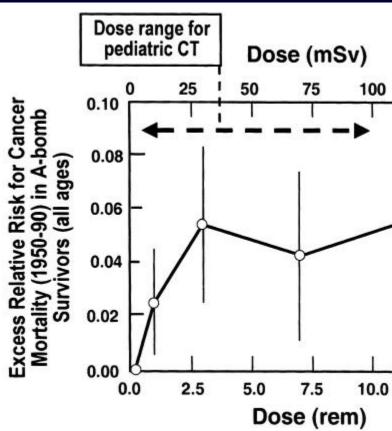
- 1. All Ages: 5%
- 2. 1st Decade: 15%
- 3. 2nd Decade: 8%
- 4. Middle Age
 - 1 2 %
- 5. Child 10 times **More Sensitive**

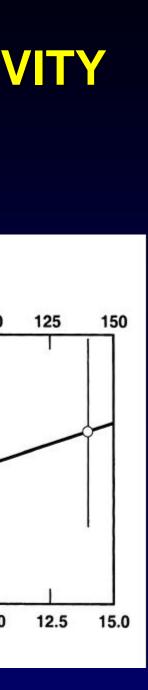


PATIENT STOCHASTIC RADIOSENSITIVITY

D. Recent A-Bomb Survivor Data

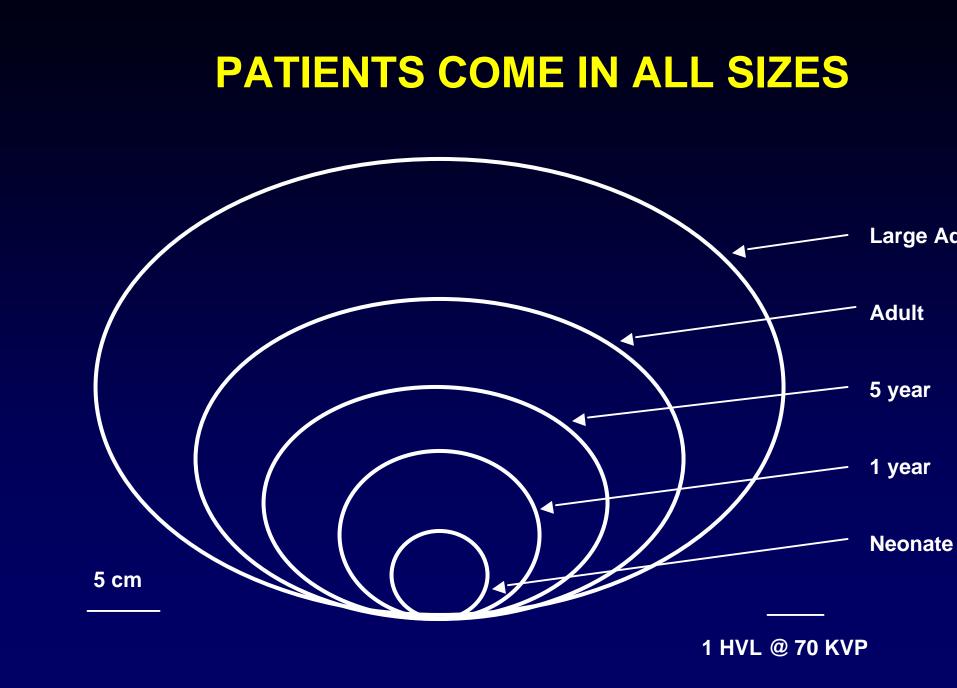
- 1. 35,000 Survivors
 - Doses > 5 rad
- 2. Received Doses Over 50 Years Ago
- 3. Statistically Significant Excess Incidence of Cancer at Nonextrapolated Doses > 3 rads





PATIENTS COME IN ALL SIZES					
		Abdominal Girth			
	<mark>(kg)</mark>	Centimeters			
Age	Mass	PA	# HVL	LAT	# H\
Neonate	2	6	2	6	2
Newborn	3	9	3	10	3
1 yr	10	12	4	14	4
5 yr	19	16	5.3	22	7
12 yr	31	18	6	27	9
Adult	68	22	7.3	33	11
Lrg Adult	130	32	10.6	48	16

VL 2 3.1 4.6 7.3 9 1 6



Large Adult

PATIENTS COME IN ALL SIZES

E. Patient Doses Below 70 kVp Are Excessive **1. Newborn Fluoro Frame** a. 70 kVp & 0.01 mAs: 0.046 mR b. 45 kVp & 0.08 mAs: 0.20 mR **2. Newborn Cath Frame** a. 70 kVp & 0.1 mAs: 0.46 mR b. 45 kVp & 0.8 mAs: 1.98 mR 3. Newborn DSA Recorded Image a. 70 kVp & 3 mAs: 14 mR b. 45 kVp & 24 mAs: 110 mR

- F. Clinical Dynamic Range of mAs per Frame to Maintain Fixed kVp
 - **1. PA Projection**
 - a. 9 Half Value Layers
 - b. Range of 512!
 - 2. LAT Projection
 - a. 14 Half Value Layers
 - b. Range of 16,000!



- **G.** Complexity
 - 1. Diagnostic Only
 - 2. Diagnostic & Interventional
 - a. Deterministic Injuries



G. Complexity Increases Deterministic Injury Risk **3.** Clinical Problems of Children are Complex a. Congenital Heart Defects and/or Diseases i. "Black Box" ii. 4 - 8 hr Exam Times **b.** 100 - 200 minutes of Fluoro Can Occur c. Malformations in Anatomy Corrected in Stages i. Up to 10 catheterizations by 21st birthday ii. Multiple interventions over weeks iii. Radiation Damage to Skin is Cumulative

IMAGING EQUIPMENT DESIGN VARIABLE RATE PULSED FLUOROSCOPY



A. Variable Rate Pulsed Fluoroscopy

- **1. Alternating if Biplane Configuration**
 - a. Scatter from Orthogonal Plane Eliminated
 - **b.** Limited Subject Contrast Maintained

2. Variable Rate

- a. 30, 15, & 7.5 pulses/sec: Cath Lab
- b. 30, 15, 7.5, 4, & 3 pulses/sec: DSA Lab
- C. 7.5, 3.75, 1.88, 1 pulses/sec: GI/GU Lab

A. Variable Rate Pulsed Fluoroscopy

3. Image Quality vs Radiation Dose

- a. Proper Pulse Width Minimizes Temporal **Information Loss**
- **b.** Pulse Width Ranges
 - i. Pediatrics: 1 5 msec
 - ii. Adults: 3 10 msec

A. Variable Rate Pulsed Fluoroscopy 3. Image Quality vs Radiation Dose c. Increased Perceived Noise Unacceptable if: i. Exposure per pulse unchanged with reduced pulse rate ii. Loss of Temporal Resolution is not the **Cause of Rejection of Variable Rate Pulsed Fluoroscopy**

- A. Variable Rate Pulsed Fluoroscopy
 - **3. Image Quality vs Radiation Dose**
 - c. Perceived Noise Compensation
 - ii. EERIR/Frame a 1/(Pulse Frequency)^{1/2}
 - Less frame integration by eye
 - EERIR/Frame Increased as Pulse Rate Decreases
 - Relationship holds above 5 pulses/sec



A. Variable Rate Pulsed Fluoroscopy

4. Tube Current

a. Minimum: 10 mA

b. Maximum: 100 mA

5. Desired Fixed High Voltage ~ 70 kV

a. Requires mAs Range of 500!

i. Too many vendors do not vary tube current and pulse width!

ii. At best have a mAs range of 50

6. 70 kVp may Occur for Only One Size Patient!



- A. Variable Rate Pulsed Fluoroscopy
 - 7. Traditional Modulation of Technical Factors
 - a. Pulse Width at Maximum
 - **b.** Tube Current
 - i. Fluoro: 50 mA
 - ii. Acquistion: Maximum Tube Loading
 - c. kVp Modulated
 - i. Minimized for Large Patients
 - ii. Excessive Dose for Small Patients



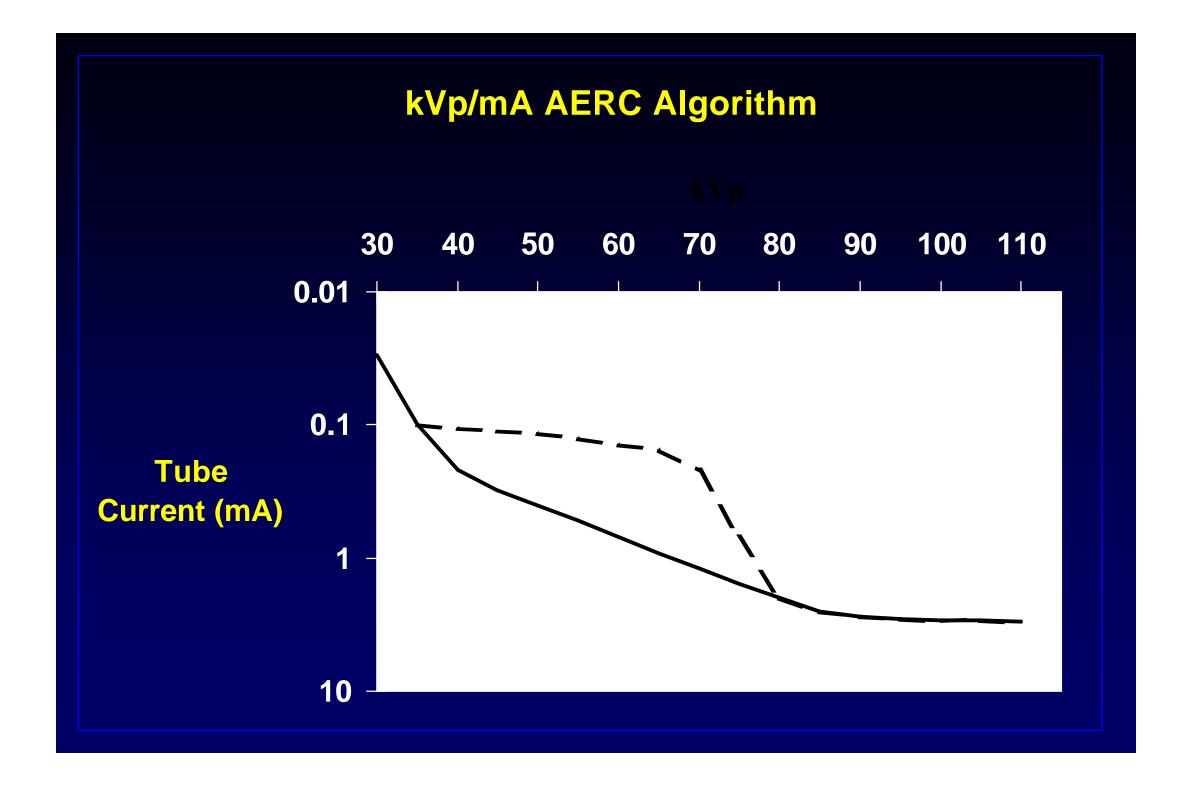
A. Variable Rate Pulsed Fluoroscopy 8. Preferred Modulation of Technique Factors a. Starting Values i. 70 kVp ii. 3 msec **b.** Modulation Hierarchy i. Tube Current ii. Pulse Width iii. High Voltage

B. Continuous Fluoroscopy
1. Preferred Technique Modulation
a. Starting kVp: 70

b. Tube Current Modulated: 0.1 - 4 mA

c. kVp Modulated Last





C. Variable Rate Radiographic Acquisitions

- 1. Cath Lab
 - a. Same Specifications as Pulsed Fluoro Except:
 - i. Variable Rate: 60, 30, & 15 pulses/sec
 - ii. Tube Current:
 - Neonate to 2 Yr: 100 mA
 - 2 12 Yr: 300 400 mA
 - 12 Yr Adult: Maximum Tube Loading
 - iii. High Voltage ~ 70 kV for Patients < 12 Yr

- **C.** Variable Rate Radiographic Acquisitions
 - 2. Vascular Lab
 - a. Variable Rate: 7.5 0.5 pulses/sec
 - **b.** Tube Current
 - i. Neonate to 2 yr: 200 mA
 - ii. 2 6 Yr: 400 600 mA
 - iii. 6 Yr Adult: Maximum Tube Loading
 - c. High Voltage ~ 70 kV for Patients < 12 Yr



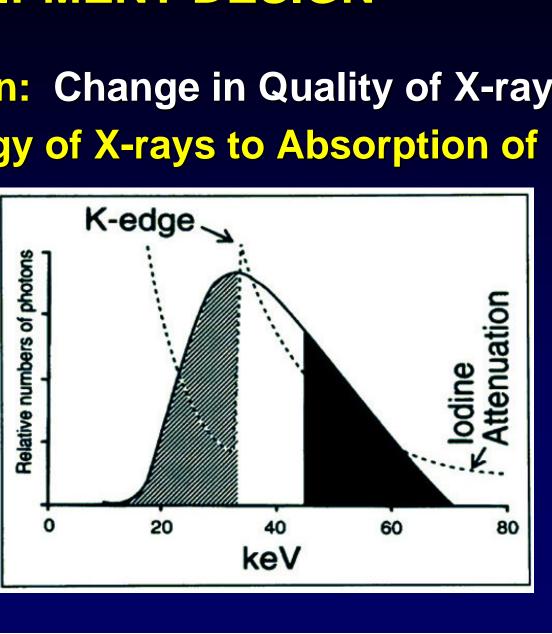
C. Variable Rate Radiographic Acquisitions **3. Preferred Technique Modulation :** a. Starting Values i. 70 kVp ii. 3 msec **b.** Modulation Hierarchy i. Tube Current ii. Pulse Width iii. High Voltage

D. Spectral Beam Filtration: Change in Quality of X-ray **Spectrum: Match Energy of X-rays to Absorption of**

Contrast Media

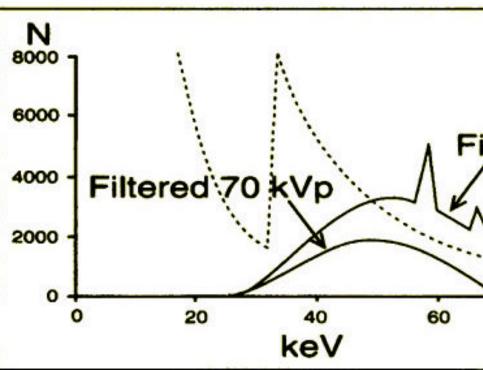
- 1. Pass 33 40 keV X-rays
- 2. Attenuate
 - a. <33 keV X-rays **Affects Dose** b. > 40 keV X-ray

Affects Contrast



D. Spectral Beam Filtration:

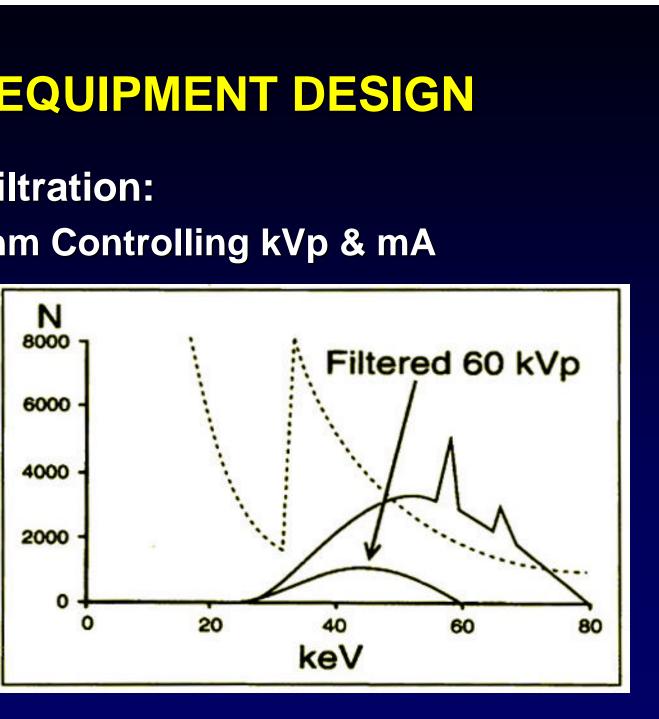
- 3. X-ray Tube Continuous Loading > 2 kW
- 4. 0.1 0.9 mm Cu Filtration
- 5. Low Energy
- Attenuated 6. kVp Increases
- 7. Excessive Effective keV



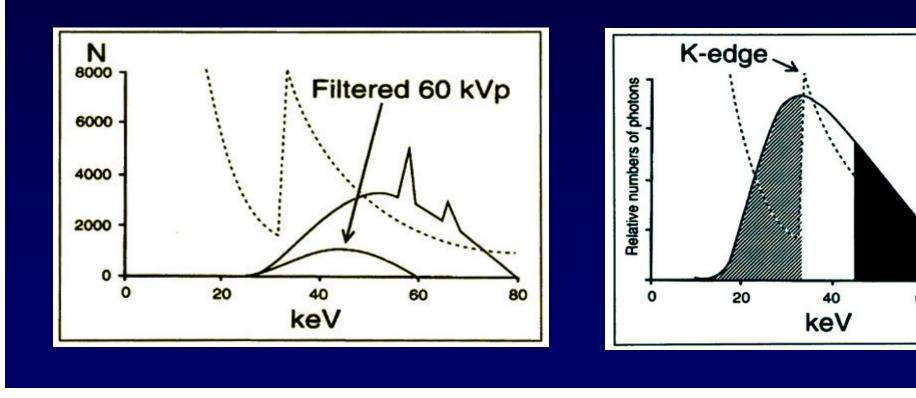


D. Spectral Beam Filtration:

- 8. Modify Algorithm Controlling kVp & mA
- 9. kVp Reduced to 60 kVp **10. X-ray Intensity Too Small**



- **D. Spectral Beam Filtration:**
 - **11. Increase mA to maximum kW**
 - 12. Adults: Fluoroscopy only \leq 0.2 mm Cu
 - 13. Pediatrics: Fluoroscopy & Radiographic





D. Spectral Beam Filtration:

14. Summary

- a. Added Filter
- **b.** Reduced High Voltage
- c. Increased Tube Current
- d. Machine should automatically select:
 - i. Thickest filter
 - ii. Resulting in 60 70 kVp
 - iii. Based on current fluoro attenuation data



E. Last Image Hold

- 1. Last Fluoroscopic Frame Stored and Continuously Displayed on TV Monitor
- 2. Poorer Quality due to Loss of Multiple Frame Integration by Eye
- 3. Allows Extended Viewing of Anatomy Without Further Radiation

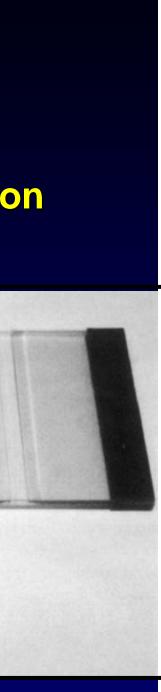


F. Fluoro Image Store

- 1. During Realtime Fluoroscopy
 - a. Frame Selected by Operator and
 - **b. Electronically Stored**
- 2. Poorer Quality due to:
 - a. Loss of Multiple Frame Integration by Eye
 - **b.** Lower Exposure at Plane of Image Receptor
- 3. Radiographic Acquisition Dose Avoided
- 4. Stored Fluoroscopic Frame Archived Electronically or on Film

Eye eptor

G. Spatial Beam Shaping 1. Equalization Filters: Attenuation Compensation a. Linear & Rotational Movement b. Tapered Lead - Acrylic Blades c. Interchangeable d. Integral Dose Reduction



G. Spatial Beam Shaping 2. Collimator Adjustment without Fluoro Radiation a. Collimator Blade Location Updated on Monitor as Blades are moved **b.** Less Dose Due to Adjustment c. Integral Dose Reduction

H. Filtration Added to X-Ray Beam **"Spectral Beam" Filtering**

- **1. Effective Energy of Beam Increases**
- 2. Less X-rays @ same EERIR
- 3. Quantum Mottle Increases for same EERIR
- 4. Double EERIR wrt Standard Filtration
- 5. EER_{filters} < EER_{std filters}

I. Electronically Adjustable Aperture in Front of TV Camera **1. Directly Controls EERIR Entrance Exposure Rate to Image Receptor** 2. Indirectly Controls EER **Entrance Exposure Rate to Patient**

- I. Electronically Adjustable Aperture
 - **3. Pulse Fluoro Frequency Change**
 - a. IIIER a 1/(Pulse Frequency)^{1/2}
 - for Pulse Frequencies > 5
 - **b.** Corrects Increased Perceived Noise due to Less Integration of TV Frames by Eye
 - c. EERIR/Frame a Constant for Pulse Frequencies < 5



I. Electronically Adjustable Aperture

4. Function of FoV Change

- a. Older Equipment With Fixed Aperture (II)
 - i. EERIR a 1/FoV²
 - ii. Corrects Loss of Minification Gain
 - iii. Maintained Brightness on Monitor
 - iv. Reduced Quantum Mottle
 - v. Significant Increase of EERIR in Mag modes



- I. Electronically Adjustable Aperture
 - 4. Function of FoV Change
 - **b.** Adjustable Aperture (II)
 - i. EERIR a 1/FoV
 - ii. Quantum Mottle (Absolute Noise) **Independent of FoV**
 - iii. Perceived Noise Increases with Sharper Image of Reduced FoV
 - iv. Correct with Increased EERIR
 - v. Less Increase of EERIR in Mag modes





- I. Electronically Adjustable Aperture
 - 4. Function of FoV Change
 - c. Adjustable Aperture Opened in Mag Modes
 - i. Conventional Image Intensifiers
 - ii. EERIR a Constant
 - iii. Increases in Perceived Noise Must be **Tolerated by Operator**
 - iii. Perceived Noise Increases with Sharper Image of Reduced FoV
 - iv. Patient Dose is Unchanged

I. Electronically Adjustable Aperture

- 4. Function of FoV Change
 - d. Flat Plate Image Receptors
 - i. EERIR a Constant
 - ii. Sharpness Minimally Affected by FoV
 - Determined by Size of Plate's Pixels
 - iii. Perceived Noise is Constant
 - iv. Patient Dose Should be Unchanged

- I. Electronically Adjustable Aperture
 - **5. Operator Selectable EERIR:**
 - **Task Oriented**
 - a. Low (Half of Medium)
 - b. Medium
 - c. High (Double Medium)



I. Electronically Adjustable Aperture				
5. Operator Selectable EERIR:				
d. Manufacturer Dependent				
e. Flat Plate Receptor Example (20 cm				
Parameter	Vendor A	Vendor B		
Low EERIR (mR/m)	5.5	9.2		
Low EER (R/m)	2.1	2.8		
Nor EERIR (mR/m)	14	7.4		
Nor EER (R/m)	5.8	4		

girth)

A. Why Acceptance Testing?

- 1. Identify & Eliminate Faulty Components
- 2. Insure Proper Setup of Equipment

a. Clinical Choices

- i. Clinical Requirements
- ii. Design Features of Equipment
- **b.** Measurement Techniques
 - i. Test Equipment Available
 - ii. Design Requirements of Clinical Unit



B. What Should be Measured?

- **1. Entrance Exposure Rate to Image Receptor**
 - a. All Fluoroscopic Modes
 - **b.** All Recording Modes
- 2. Entrance Exposure Rate to Patient
 - a. Maximum
 - **b.** All Patient Sizes to be Imaged
- 3. Do Not Assume Installer has Addressed These Issues!!!!

C. Appropriate Performance Levels?

- 1. EERIR_{variable}
 - a. EERIR/Fr = (EERIR₃₀/Fr) / (Pulse Frequency)^{1/2}
 - **b.** $EERIR_{spectral filter} = 2 \times EERIR_{std filter}$
 - c. EERIR a 1/FoV²
 - d. EERIR a 1/FoV
 - e. EERIR a Constant (function of FoV Flat Plate)
 - f. $1/2 \times EERIR_{high} = EERIR_{normal}$
 - g. $EERIR_{normal} = EERIR_{low} \times 2$

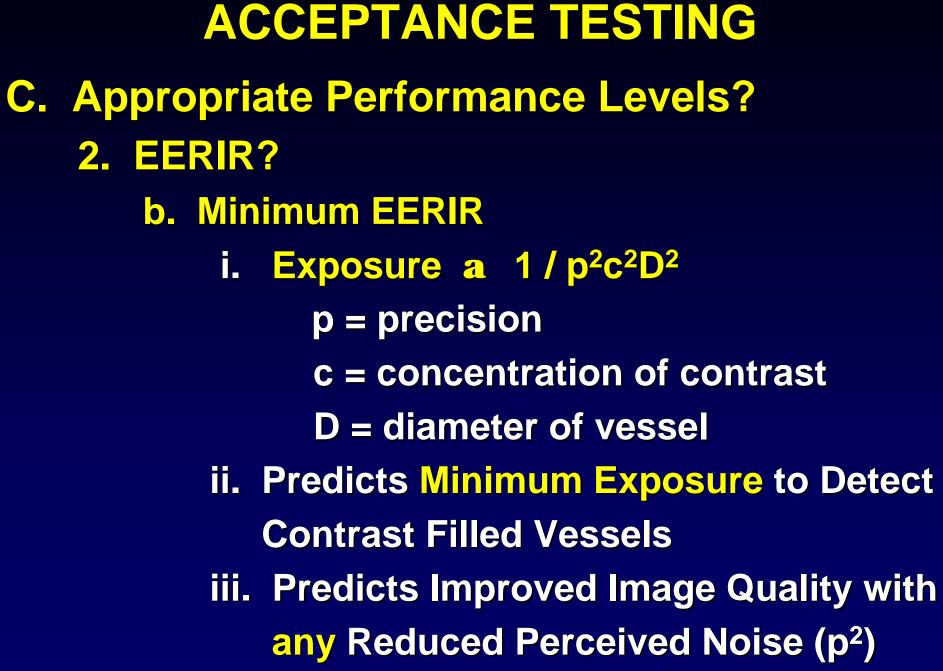
C. Appropriate Performance Levels?

- **2. EERIR?**
 - a. Set EERIR to Provide Adequate Image Quality

b. Minimum EERIR

- i. Equipment Design
- ii. Image Quality Requirements
 - Diameter of Vessel
 - Concentration of Contrast Material





C. Appropriate Performance Levels? **2. EERIR?**

c. Maximum EERIR

- i. Perceived Noise a Function of System Noise
- ii. System Noise = $[QM^2 + EN^2]^{0.5}$
 - QM = Quantum Mottle
 - **EN = Electronic Noise**

C. Appropriate Performance Levels? **2. EERIR?**

- c. Maximum EERIR
 - iii. Want QM < EN
 - iv. When QM = EN Further Increases in **EERIR** are Wasted
 - v. Excessive EERIR Degrades Image Quality
 - 10 R/min Limit
 - Loss of Brightness on TV Monitor



Entrance Exposure Rate to Image Intensifier 22 cm FOV @ 80 kVp **Standard Filtration & kVp/mA Power Curves 30 Pulses per Second <u>Operational Mode</u> <u>EERII Range (µR/frame)</u>** Standard Fluoroscopy 1.5 - 2.5

High Dose Fluoroscopy 3 - 6 **Digital Angiography** Digital Subtraction Angio 500 - 1000 **Cardiac Digital Cine Film**

50 - 100 8 - 10 10 - 15



- **C.** Appropriate Performance Levels? **2. EERIR?**
 - d. FPDER: Flat Plate Detector Exposure Rate
 - i. Standard Filtration & kVp/mA Power Curves
 - ii. 20 cm FOV @ 80 kVp
 - iii. 30 Pulses per Second

Operational Mode

EERIR Range (µR/frame)

Standard Fluoroscopy Digital Angiography **Cardiac Digital**

2.5 50 - 100 10 - 15

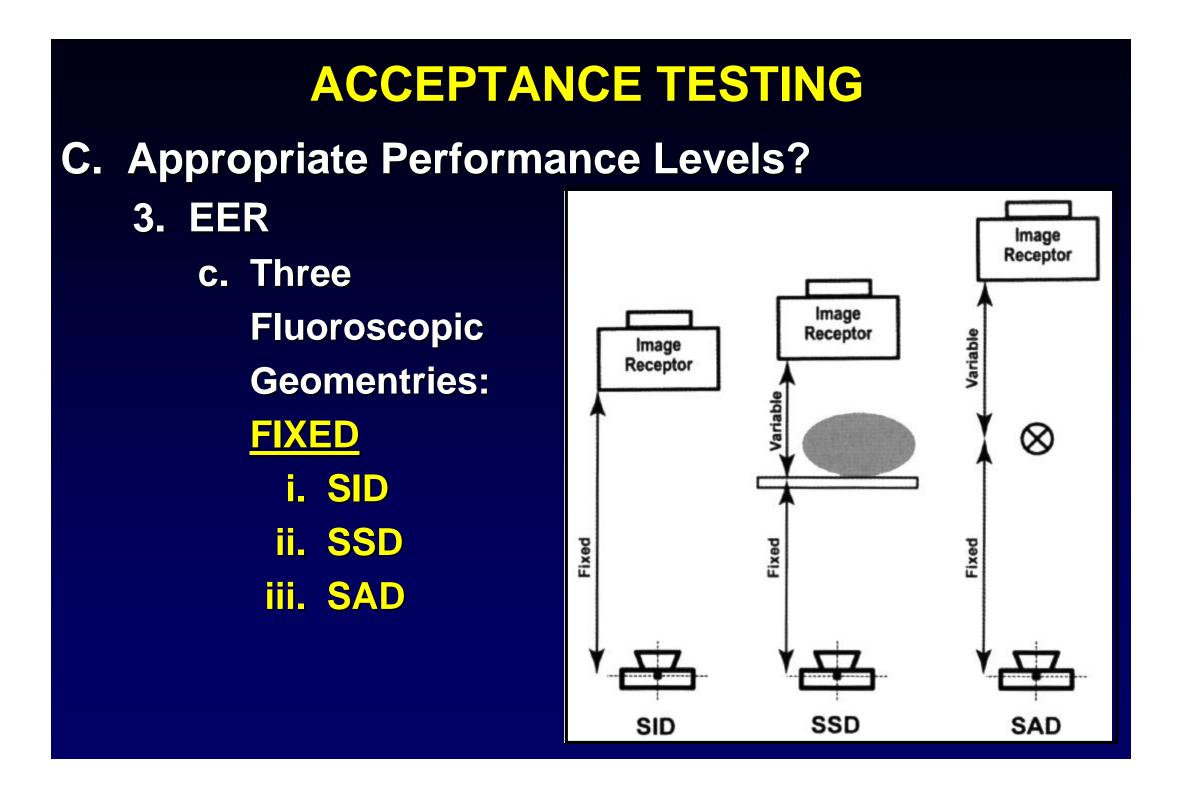


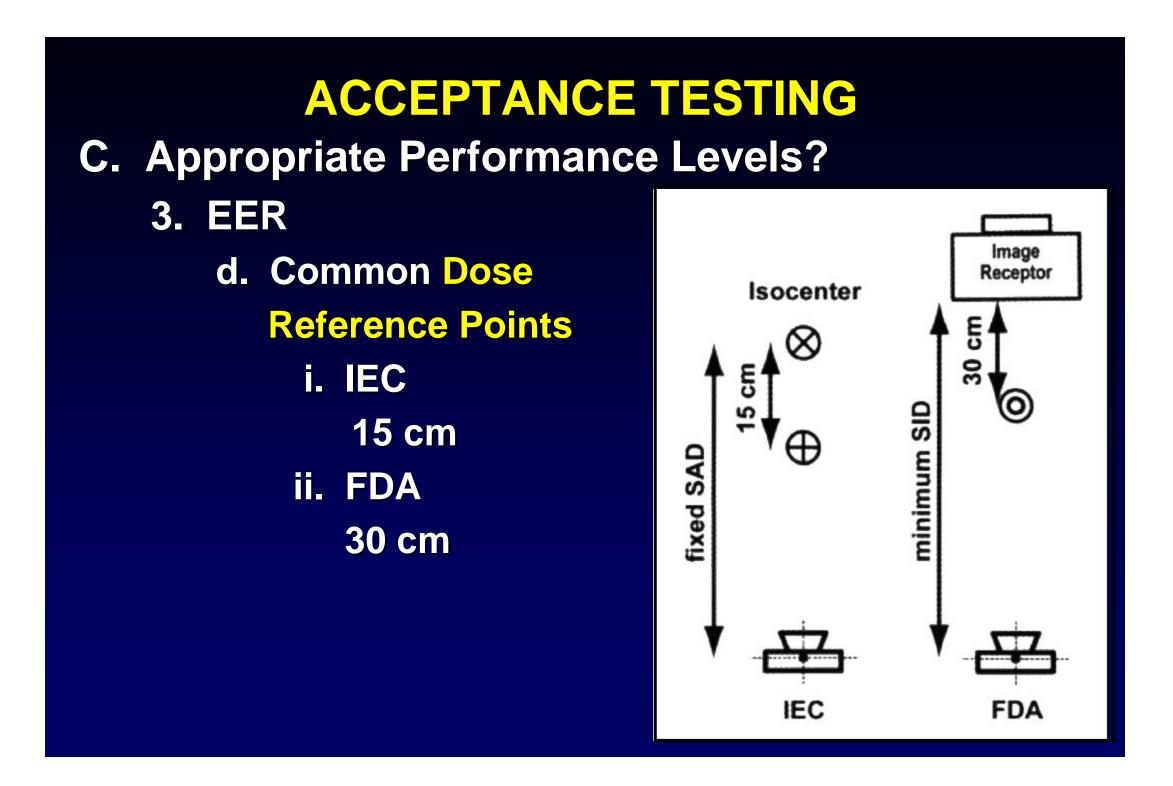
- C. Appropriate Performance Levels? 2. EERIR?
 - d. FPDER: Flat Plate Detector Exposure Rate
 - iv. Unchanged as FoV changes
 - v. Justification
 - Measured Sharpness of image basically independent of FoV
 - Sharpness of image similar to 5" FoV II



- C. Appropriate Performance Levels?3. EER?
 - a. Entrance Exposure Rate
 - b. Where?
 - i. Patient's Skin?
 - ii. Reference Point?







- C. Appropriate Performance Levels?3. EER
 - e. Other Important Parameters
 - i. a mA
 - ii. a kVp²
 - iii. ~ a ~ EERIR
 - Added Filtration
 - Beam Shaping Filters
 - Grid Factors



C. Appropriate Performance Levels? 3. EER e. Other Important Parameters

iv. Function of Patient Size

v. a $(1 / distance)^2$



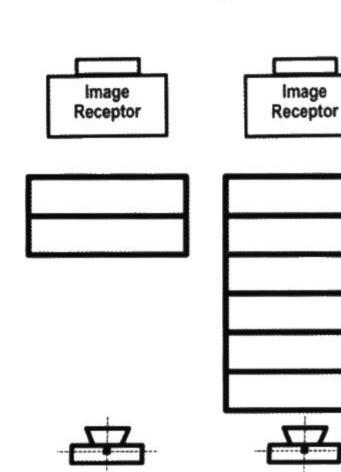
C. Appropriate Performance Levels?

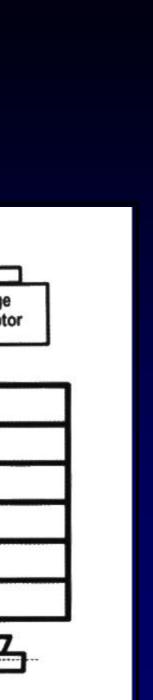
4. Affect of Increasing

Patient Size

- a. Fixed SID
 - i. Attenuation?
 - ii. Shorter

SSD?





C. Appropriate Performance Levels?

4. Affect of Increasing

Patient Size

- **b.** Fixed SSD
 - i. Attenuation?
 - ii. Longer

SID?

	Im Rec
Image Receptor	

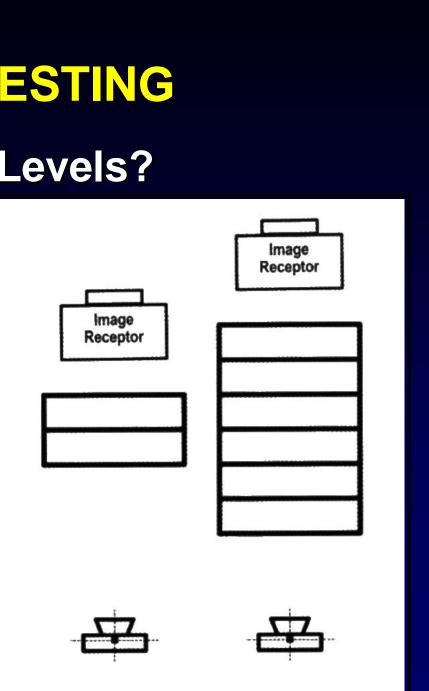






C. Appropriate Performance Levels?

- 4. Affect of Increasing
 - Patient Size
 - c. Fixed SAD
 - i. Attenuation?
 - ii. Longer
 - SID?
 - iii. Shorter SSD?



D. Measurement Pitfalls

- 1. Dosimeter
 - a. Constant Energy Response
 - i. 50 120 kVp
 - ii. 2 14 mm Al HVL
 - b. Collection Efficiency 95% @ 2,000 - 10,000 R/min
 - **c.** Leakage < 1 x 10⁻¹⁴ Amp



1. Dosimeter

- d. Shape of Ionization Chamber
 - i. Parallel Plate
 - Fits behind Grids
 - High Collection Efficiency
 - X-ray "Transparency"
 - ii. Cylindrical
 - No Directional Response



D. Measu	urement Pitfal	S		
2. Attenuation Phantom Materials				
Material	Effective Z	Density	BE(ke	
Water	7.4	1.00	0.5	
PMMA	6.6	1.19	0.5	
AI (1100)	13	2.70	1.6	
Copper	29	8.93	9.0	



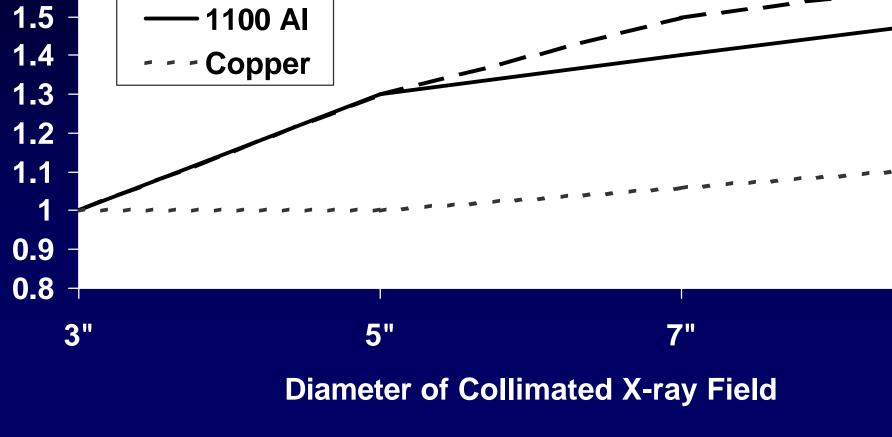
- **D. Measurement Pitfalls**
 - 2. Attenuation Phantom Materials
 - **b.** Required Phantom Material Thickness
 - i. Water: 25 cm
 - ii. PMMA: 25 cm
 - iii. Aluminum: 7.6 cm
 - iv. Copper: 0.8 cm

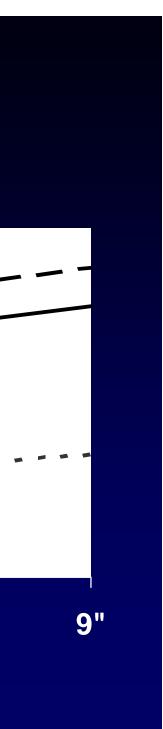


D. Measurement Pitfalls

- 3. Scatter/Primary Ratio
 - a. PMMA
 - b. 1100 Alloy Aluminum
 - c. Copper







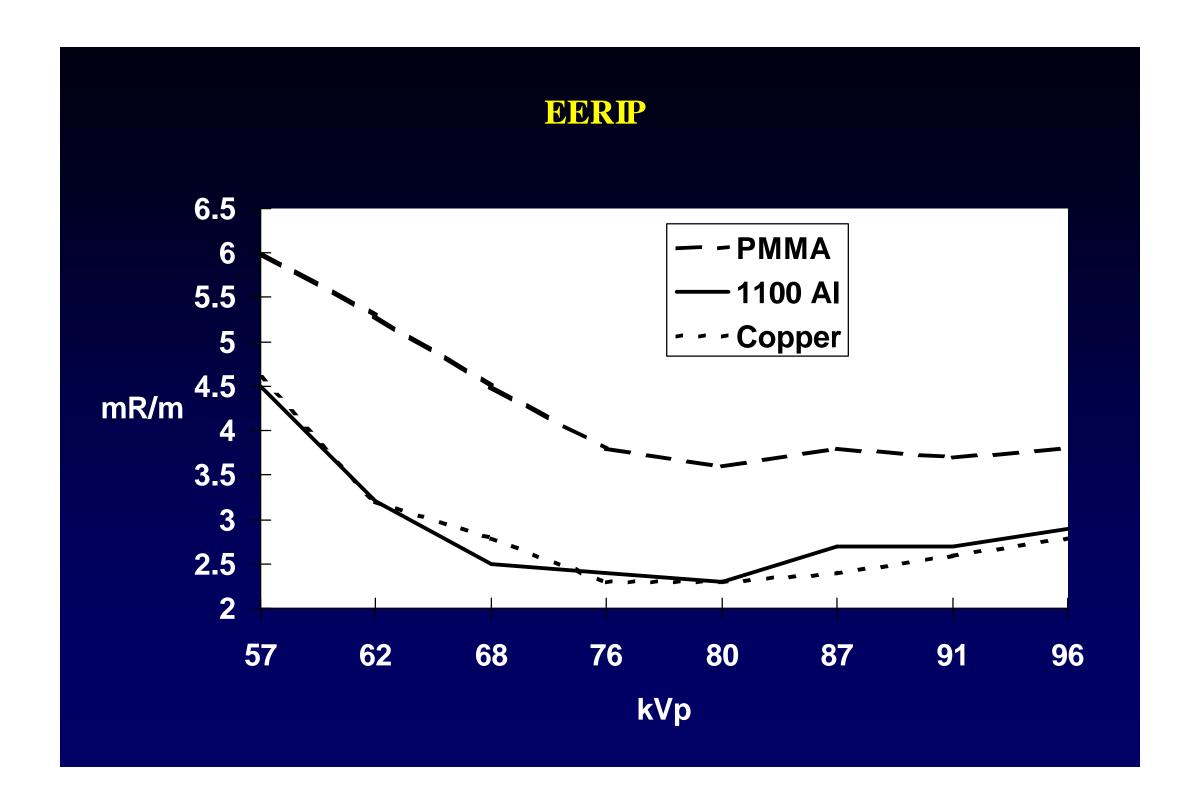
ACCEPTANCE TESTING

D. Measurement Pitfalls

4. Affects of Effective Energy

- a. HVL_{23 cm water} ~ HVL_{0.5 mm Cu}
- **b. Measured EERIR Differences**
 - i. EERIR_{AI} ~ EERIR_{Cu}
 - ii. $EERIR_{PMMA} \sim 1.5 \times EERIR_{Cu}$





A. Comprehensive Training Fosters

- 1. Full Utilization of Equipment Design
- 2. Optimum Image Quality 3. Reduced Radiation Dose



B. Types of Training

- 1. Core Knowledge Provided at Regular In-Services
 - a. Basic Imaging Principles
 - **b.** Quality Control Responsibilities
 - c. Equipment Care & Maintenance
 - d. Radiation Protection Principles



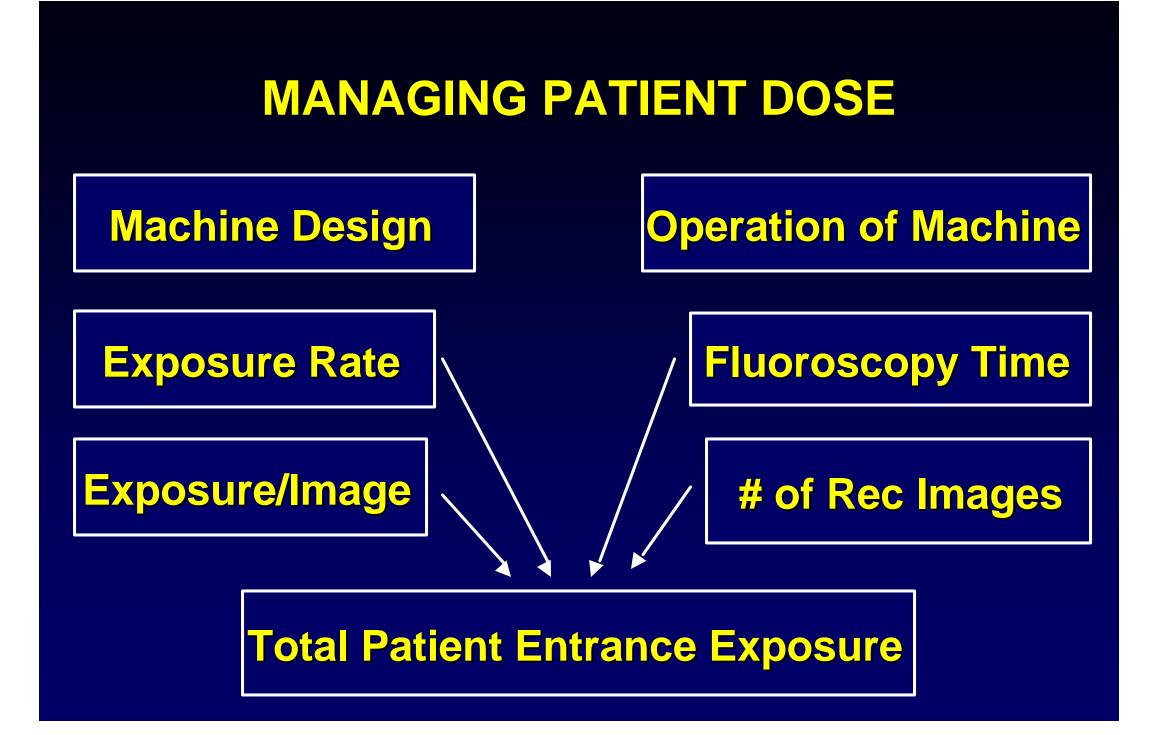
- **B.** Types of Training
 - 1. Core Knowledge
 - d. Radiation Protection Principles
 - i. Principles of X-Ray Production
 - ii. Patient/Operator Geometries
 - iii. Appropriate Use of Shielding Devices
 - iv. Credentialling Program



B. Types of Training

- 2. "Buttonology": Unique Operational Features of Imaging Equipment
 - a. Establish Lead Operators
 - **b.** Other clinical sites
 - c. Vendor's headquarters
 - d. Phantom Imaging on Site
 - e. First patients





A. GOALS

- 1. Allows Informed Risk-Benefit Decisions During Study
- 2. Document Individual Clinical Exposures
- 3. Allows Management of:
 - a. Radiation Risks to Patients and Personnel
 - **b.** Changes in Equipment Performance

s onnel

B. Additional Reading

Balter S, Shope TB, Fletcher DW, Kuan HM, Seissl H. "Techniques to Estimate **Radiation Dose to Skin During Fluorosopically Guided Procedures**" **1992 AAPM Summer School Proceedings**



B. What is the Best Indicator of Patient Risk?

- **1. Historical Measurements Limited by Available Instrumentation**
 - a. Fluoroscopy Time
 - **b.** TLD Skin Dose Measurements
 - c. Cumulative Skin Dose
 - d. Peak Skin Dose



C. Fluoroscopy Time Limitations

- **1. Fluoro Dose Rates Vary Over Wide Range**
 - a. Patient Size
 - b. kVp
 - c. mA
 - d. Beam Orientation
 - e. FoV
 - f. Source Skin Distance
 - g. Spectral Beam Filtration
- 2. Dose from Recorded Images Ignored



D. Cumulative Dose

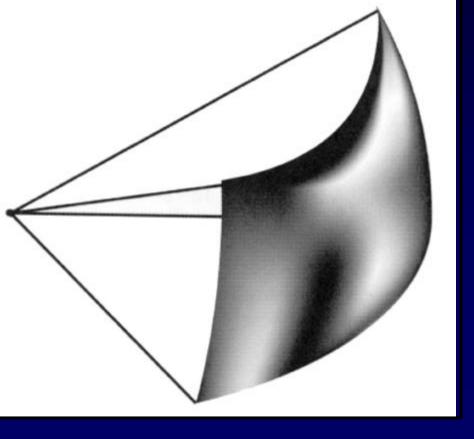
- 1. Total Dose Delivered During Exam
- 2. Can be Measured Real-Time
- **3. Indirect Measurement**
 - a. Estimates Dose at Reference Point
 - b. Based on Direct Measurements at Other Locations



D. Cumulative Dose

4. Dose-Area-Product (DAP)

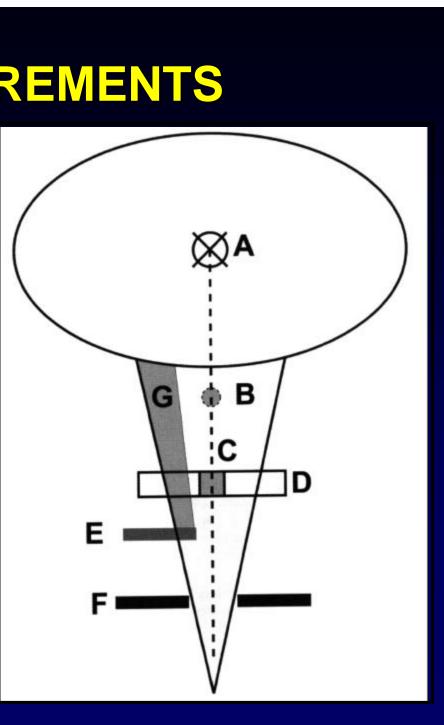
- a. Integral of Dose
 Across Entire
 X-Ray Beam
 b. Estimates Upper
 - Limit of Total Energy Absorbed by Patient





D. Cumulative Dose4. DAP

- a. Isocenter
- **b.** Dose Reference Point
- c. KERMA chamber
- d. DAP chamber
- e. "Wedge" Filter
- f. Collimator Blade
- g. Reduced Dose Area



D. Cumulative Dose **4. DAP**

c. Advantages

- i. Simple Installation & Calibration
- ii. Independent of Distance From **Focal Spot**
- iii. Teaching Tool of Scatter Production
- iv. Indication of Integral Dose

- **D.** Cumulative Dose
 - **4. DAP**
 - c. Disadvantages
 - i. No Correction for Table Top Attenuation
 - ii. Source to Skin Distance?
 - iii. Spatial Distribution of Entrance Beam?
 - iv. Overestimates Possibility of Exceeding **Deterministic Threshold**
 - v. Inaccurate Skin Dose Estimations



D. Cumulative Dose 5. Derived Patient Exposure a. Exposure Rate and b. Cumulative Exposure to Reference Point From Real-Time Data Within X-ray System

- **D.** Cumulative Dose
 - 5. Derived Patient Exposure
 - c. Required Data
 - i. KiloVoltage
 - ii. Tube Current
 - iii. Time
 - iv. Source Skin Distance
 - v. Calibration Algorithms
 - vi. Patient Support Attenuation



- **D.** Cumulative Dose
 - 5. Derived Patient Exposured. PEMNET®



- i. Advantages
 - 5% Accuracy
 - Database Provided
 - Real-Time Displays



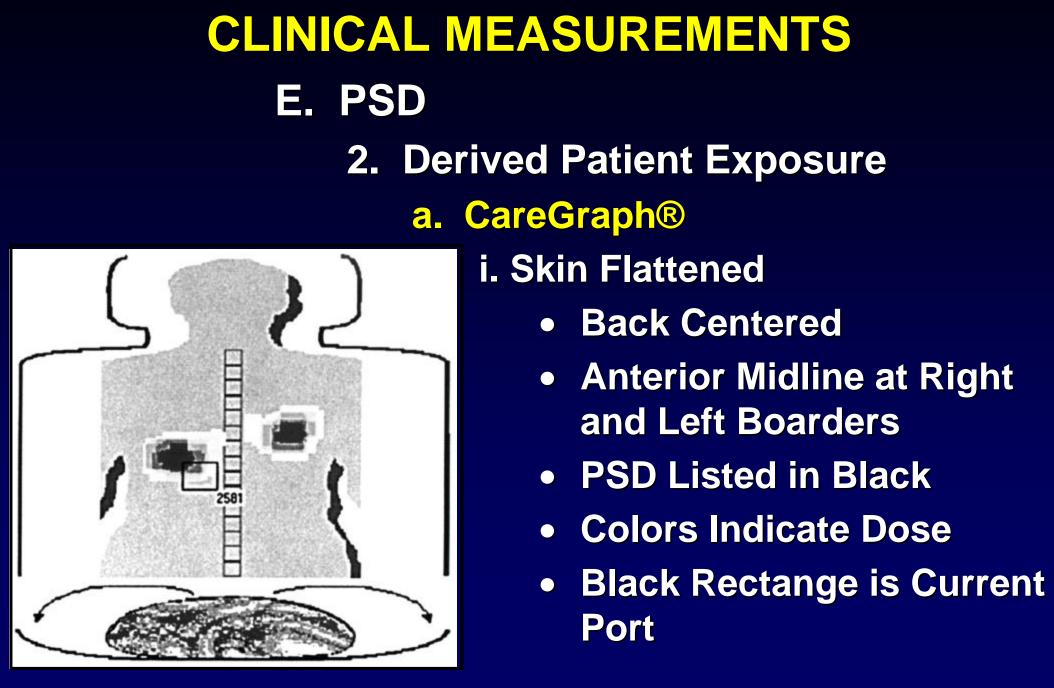
- **D.** Cumulative Dose
 - **5. Derived Patient Exposure**
 - d. **PEMNET**®

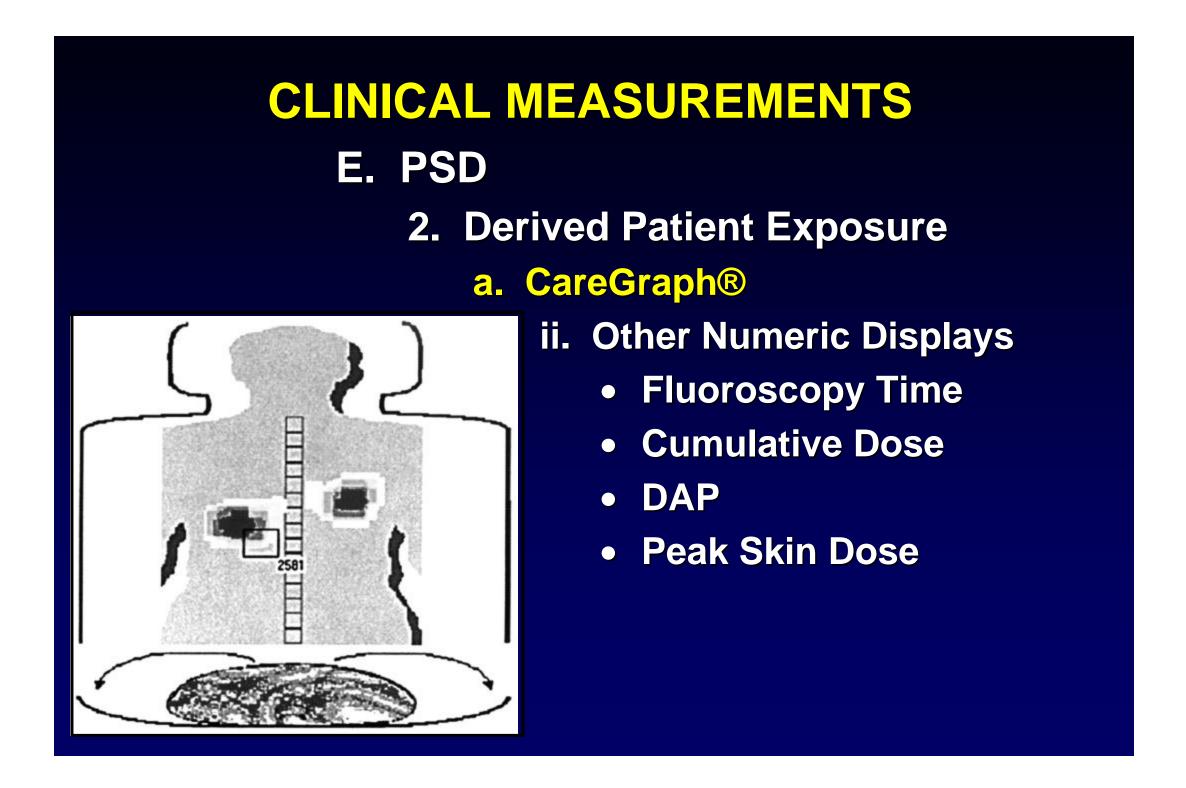


- i. Disadvantages
 - Additional Cabling
 - Noise Free Interfaces
 - Involved Calibration
 - Database Maintenance
 - Spatial Distribution of **Entrance Beam?**

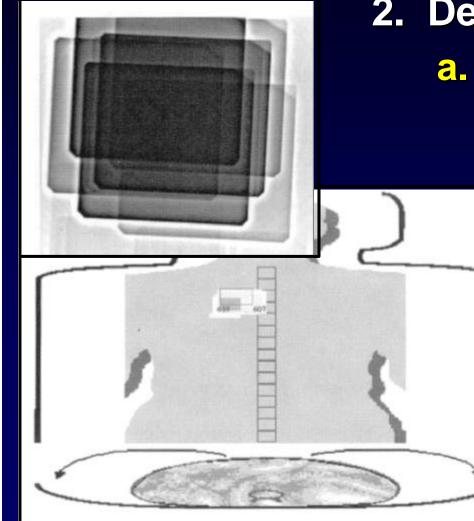
CLINICAL MEASUREMENTS E. Peak Skin Dose (PSD) 1. Peak Skin Dose ? Cumulative Dose a. Entrance Port Moves During Exam i. Beam Orientation ii. Field of View **b.** Dose for Given Port i. On-Time ii. Intensity • Patient Size Beam Orientation c. Overlap of Ports



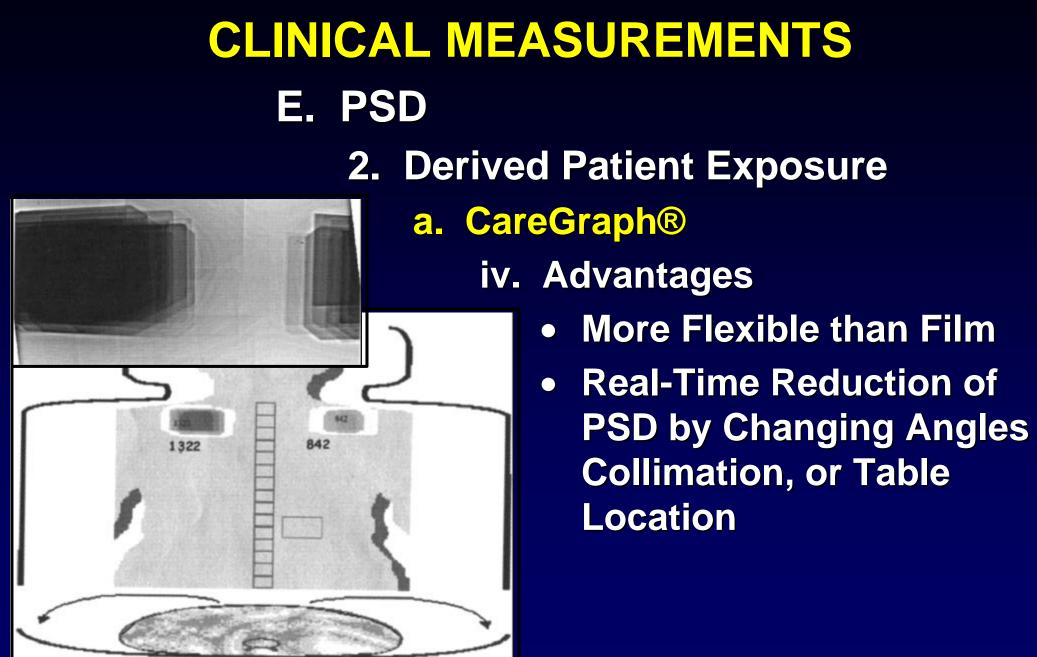




CLINICAL MEASUREMENTS E. PSD



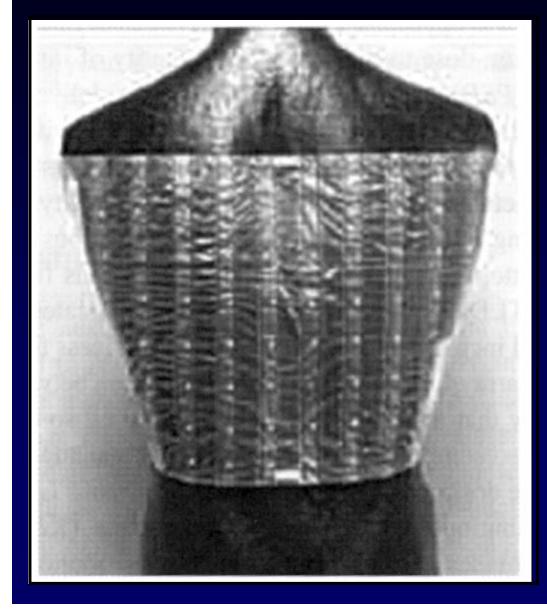
- 2. Derived Patient Exposure
 - a. CareGraph®
 - iii. Disadvantages
 - No Longer Available
 - Skin Modeled to One **Standard Adult Body**
 - Information from **Individual Ports is More** Limited than Film

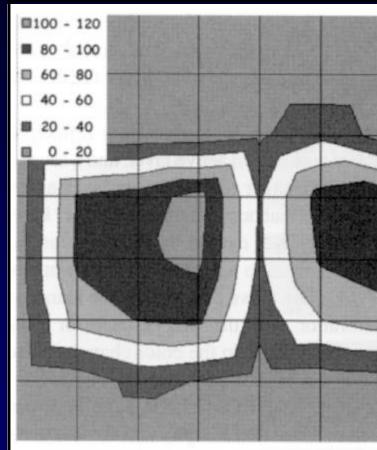


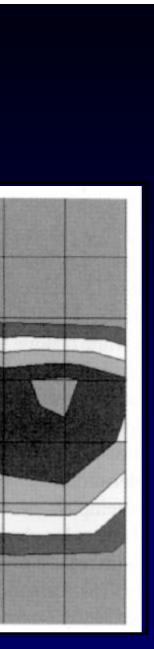
F. Other Direct Measures of Skin Dose

- 1. Thermoluminescent Dosimetry (TLD)
 - a. Advantages
 - i. Small Size
 - ii. Are Not Imaged
 - **b. Disadvantages**
 - i. Post Exposure Processing Required
 - ii. No Real-Time Feedback to Operator
 - iii. Location of PSD Must be Known

ed or

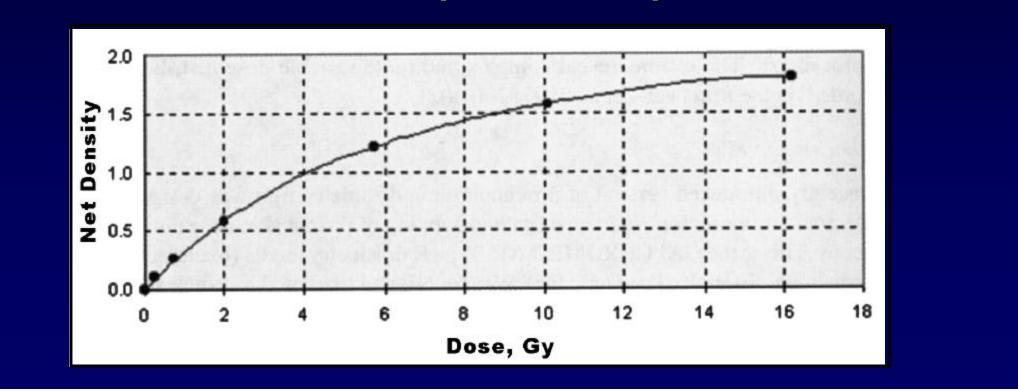




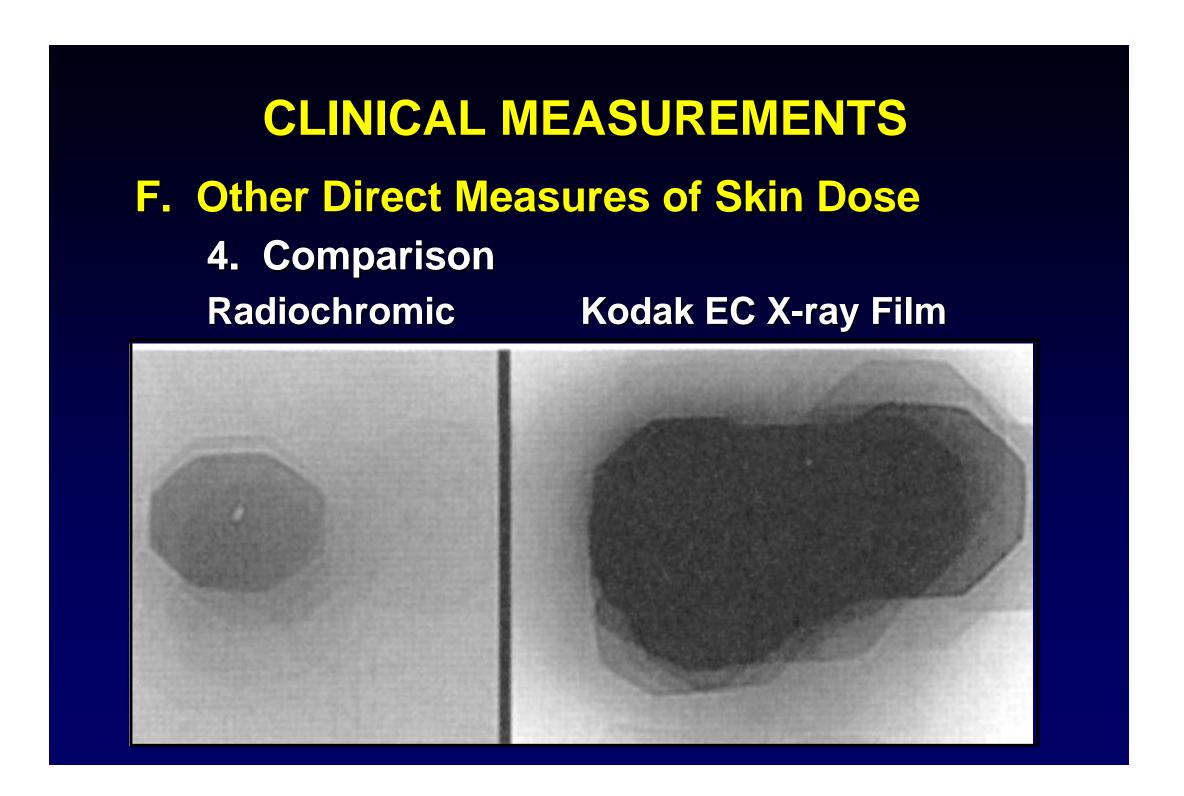


CLINICAL MEASUREMENTS
F. Other Direct Measures of Skin Dose
2. X-Ray Film Dosimetry
a. Advantages
i. Dose Distribution Illustrated
ii. Can be Used with any X-ray Unit
iii. Can Provide Quantitative Dose Info
b. Disadvantages
i. Limited Range
ii. Factors Affecting Film Sensitivity
iii. Positioning wrt to the patient
iv. No Real-Time Feedback

- F. Other Direct Measures of Skin Dose
 - 3. Radiochromatic Film (GAFCHROMIC XR-Type R)
 - a. Chemical Radiation Sensors that Change Color in Response to Exposure



<mark>Type R)</mark> ange



CONCLUSIONS

A. Verify Optimized Imaging Parameters

- 1. Image Quality will be improved
- 2. EERIP may be lowered
- 3. EER to Patient may be lowered

B. Monitor Clinical Exposures

- **1. Informed Proactive Risk Benefit Decisions**
- **2.** Patient Exposures Documented
- **C.** Physicist Must Understand:
 - **1. Imaging System Design and its Limitations**
 - 2. Clinicians and Clinical Demands